

Comparative diffusion Kinetics of Lawsonia and Rubia in 'Shatadhauta Ghrita' and Aloe vera based Formulations

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Foot cracks are a common dermatological condition that require intensive and long-term care for effective management. Ayurvedic Shatadhauta Ghrita, a lipid-rich base, is known to enhance skin permeation and provide sustained soothing effects. The present study focuses on the use of Shatadhauta Ghrita as a base incorporated with herbal extracts of Lawsonia inermis and Rubia cordifolia, and compares its transdermal diffusion performance with Aloe Vera gel-based formulations. Diffusion studies were carried out using both synthetic and biological membranes over a period of 300 minutes employing Franz diffusion cells. Simultaneous analysis of the metabolites was determined using dual wavelength UV spectroscopy. The results demonstrated that Lawsonia and Rubia metabolites exhibited significantly higher cumulative drug release, flux, and permeability from the Ghrita-based formulations, particularly through the biological membrane. Kinetic analysis suggested a controlled, erosion-assisted diffusion mechanism for Lawsonia, while Rubia showed sustained Fickian diffusion from the lipid-rich base. An increased lag time was observed for Lawsonia, whereas Rubia exhibited moderate lag characteristics in the Ghrita formulation through the biological membrane. Overall, Shatadhauta Ghrita demonstrated superior enhancement of transdermal diffusion for both hydrophilic Lawsonia and lipophilic Rubia constituents, supporting its potential as an effective base for herbal foot crack management.

Keywords: Franz diffusion study; Lawsonia; Permeation release study; Rubia; Shatadhauta Ghrita; Transdermal diffusion.

Cracked feet are common problem often caused by lack of moisture, harsh weather, standing for long period, medical condition like diabetes, which can cause bleeding, pain, discomfort and secondary infections.¹ Although conventional topical formulations provide symptomatic relief, their long-term application is often limited by the presence of synthetic excipients, which may provoke irritation or hypersensitivity reactions.

This has led to increased interest in natural and herbal alternatives that are both safe and effective in promoting sustained skin repair.²

In this context, a novel foot crack cream was developed using the *Shatadhauta Ghrita*, a traditional Ayurvedic preparation made by washing ghee hundred times with water.³ It's moisturizing, calming and wound healing qualities as well as skin penetrating properties make it excellent base for

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treating cracked heels.⁴ For further enhancement of this base ethanolic extract of Henna and Manjistha were added to make it more potent and effective to repair cracked heels.

Henna is a plant known as *Lawsonia inermis* Linn. belonging to Lythraceae. It contains active compounds like lawsone (2-hydroxy-1,4-naphthoquinone), alkaloids, proteins, terpenoids, quinines, coumarins, flavonoids, and saponins.^{5,6} It has been traditionally used for various skin conditions like fungal infections, seborrheic dermatitis, burns and to aid in wound healing. In Asian countries henna paste is applied to the hands, hair and feet. Its cooling and soothing properties help calm irritated skin, while its ability to stimulate epithelial regeneration supports tissue repair.^{7,8}

Manjistha, known as *Rubia cordifolia* Linn. belonging to Rubiaceae. It is a well-known herb in Ayurveda, traditionally used for blood purifying, and detoxifying properties.⁹ Traditional Ayurveda uses it as a natural dye for fabrics and herbal cosmetics. Its major bioactive constituents are rubiadin, purpurin, munjistin, including xanthopurpurin, triterpenoids, flavonoids, and tannins. These compounds contribute to its wide range of pharmacological actions, such as anti-inflammatory, anti-microbial, antioxidant, and anti-bacterial effects. It helps to treat skin disorders, remove toxins, and promote wound healing and tissue regeneration, making it effective in formulations for repairing cracked or damaged skin.¹⁰⁻¹²

To investigate the dermal permeation potential of both plants bioactive like Lawsone and rubiadin, a Franz diffusion study were performed comparing *Shatadhauta Ghrita* based and Aloe Vera gel based formulations by using synthetic and biological membranes.

In this research work, simultaneous analysis of the diffusion profiles of *Lawsonia* and *Rubia* extracts were performed using UV spectroscopy at dual wavelength mode. The cumulative released metabolites were further analyzed using various kinetic models. This comparative approach provided insight into the permeation efficiency of the herbal actives and also highlighted the functional superiority of *Shatadhauta Ghrita* as a transdermal delivery enhancer in herbal foot care.

MATERIALS AND METHODS

Crude plant powder of Henna (*L. inermis*) and Manjistha (*R. cordifolia*) collected from local store (Dagduteli Kashtashaudhi), Nashik. Cow's ghee, Aloe Vera gel, Glycerin, Tea Tree oil, Sodium Benzoate, and Ascorbyl palmitate, Disodium hydrogen phosphate, Potassium dihydrogen phosphate, Sodium chloride, Ethanol 95 %, Distilled water.

Standard- Lawsone, Yucca Enterprises (Batch no. 83-72-7)

Membrane: Dialysis membrane -70 (LA 393) (Dolphin, Mumbai),

Goat ear skin (Slaughter House)

Instruments: Soxhlet apparatus, UV-Visible Spectroscopy (LABINDIA Analytical, UV 3200), Franz Diffusion Cell (with receptor compartment volume: 30 mL, Diffusion area: 3.14 cm²), Make: Dolphin, Mumbai.

Sample preparation

Preparation of Plant Extracts

The powdered plant materials of Henna and Manjistha were subjected to Soxhlet extraction using ethanol, individually. The extracts were filtered, concentrated and designated as LIE for *L. inermis* extract and RCE for *R. cordifolia* extract.

Preparation of *Shatadhauta Ghrita*¹³

Shatadhauta Ghrita was prepared following traditional Ayurvedic methods by washing cow's ghee 100 times with purified water. The process involved ten thousand manual rotations in a copper vessel, with the water being decanted after every 100 rotations. This washing and decanting cycle was repeated until all 100 washes were completed. The mixture was triturated repeatedly until a smooth, cream like consistency was achieved.

Foot crack cream containing *Shatadhauta Ghrita* (Designated as FCSG) Master Formula: *L. inermis* extract (LIE) 2%, *R. cordifolia* extract (RCE) 2%, Aloe Vera gel 15 %, Glycerine 2%, Tea tree oil 1%, Ascorbyl palmetate 0.2 %, Sodium benzoate 0.1 %, *Shatadhauta Ghrita* Quantity sufficient (Q.S).

Non-*Shatadhauta Ghrita* Aloe Vera gel (Designated as NSG-AV) containing

L. inermis extract (LIE) 2%, *R. cordifolia* extract (RCE) 2%, Glycerine 2%, Tea tree oil

1%, Ascorbyl palmitate 0.2 %, Sodium benzoate 0.1 %, Aloe Vera gel quantity sufficient (Q.S).

Preparation of Buffer Solution (Phosphate Buffer pH 6.4) as per I.P 2022

Phosphate buffer of pH 6.4 was prepared by dissolving 1.79 g of disodium hydrogen phosphate, 1.36 g of potassium dihydrogen phosphate and 8.0 g of sodium chloride in distilled water and the volume made to 1000 mL in a volumetric flask. The pH was checked and adjusted, if necessary, using dilute NaOH or HCl. This buffer solution was used as the solvent for the preparation of standard and sample solutions, as the blank for UV analysis and for Franz diffusion study.

Determination of λ_{max} and Calibration curve for *L. inermis* extract using Standard Lawsone

To determine the maximum absorbance wavelength (λ_{max}) of Lawsone, a standard solution of 100 $\mu\text{g/mL}$ was prepared in phosphate buffer (pH 6.4). The solution was scanned in the UV-Spectroscopy over a range of 200–700 nm using phosphate buffer as the blank. The λ_{max} was found to be 452 nm, which was used for all further UV absorbance measurements.

From this stock solution, serial dilutions were prepared to obtain concentrations ranging from 5 to 25 $\mu\text{g/mL}$ the absorbance of each solution was measured at 452 nm using a UV-Visible spectrophotometer. A calibration curve of absorbance versus concentration was plotted, and the linear regression equation was derived to quantify Lawsone content in the test samples of diffusion study.

Determination of λ_{max} and calibration curve for Rubiadin in *R. cordifolia* extract

To determine the maximum absorbance wavelength (λ_{max}) of Rubiadin in *R. cordifolia* extract, a standard solution of 100 $\mu\text{g/mL}$ was prepared in phosphate buffer (pH 6.4) and scanned in the UV- Spectroscopy in the wavelength range of 200–700 nm using the buffer as blank. The maximum absorbance (λ_{max}) was observed at 322 nm, which was used for all further analysis.

From this stock solution, serial dilutions were prepared to obtain concentrations ranging from 60 to 100 $\mu\text{g/mL}$ the absorbance of each solution was measured at 322 nm using a UV-Visible spectrophotometer. A calibration curve of absorbance versus concentration was plotted,

and the linear regression equation was derived to quantify *R. cordifolia* extract content in the test samples of diffusion study.

Drug diffusion Study Using Franz Diffusion Cell apparatus¹⁴

Preparation of Membranes

A. Dialysis Membrane: Commercial dialysis membrane was cut in round shape of Diameter 30 mm and soaked in phosphate buffer (pH6.8) 24 hr.

Franz Diffusion Cell Setup

Franz diffusion cells have an effective diffusion area of 3.14 cm^2 . The receptor compartment was filled with phosphate buffer pH 6.4 and maintained at $37 \pm 0.5^\circ\text{C}$. Continuous stirring was done with magnetic stirrer of Dolphin cell.

Mounting of Membranes

Dialysis Membrane: Clamped between donor and receptor compartments with no air bubbles.

Goat Ear Skin: Mounted with the stratum corneum facing the donor compartment.

Four sets of cells are mounted as follows: Cell 1 and 3: Dolphin dialysis membrane; Cell 2 and 4: Goat ear skin.

Sample Application

500 mg Foot Crack Cream *Shatadhauta Ghrita* based (FCSG) and 500 mg Non-Shatadhauta Ghrita Aloe Vera gel (NSG-AV) were applied separately to donor compartments as follows.

Cell 1: Dialysis membrane - FCSG is applied,

Cell 2: Goat ear skin - FCSG is applied,

Cell 3: Dialysis membrane -NSG- AV is applied,

Cell 4: Goat ear skin - NSG- AV is applied.

Sampling

At 0, 1, 2, 3, 4, and 5 hours, 1 mL of sample was withdrawn from the receptor compartment and replaced with 1mL of fresh phosphate buffer pH (6.4). Withdrawn 1mL sample diluted with fresh Phosphate buffer pH (6.4) up to 3mL in glass stoppered test tube.

Simultaneous Analysis and kinetic modeling¹⁵⁻¹⁷

Samples were analyzed simultaneously at two λ_{max} , 452 nm for Lawsone of *L. inermis* extract (LIE) and the 322 nm for *R. cordifolia* extract (RCE) in UV spectroscopy by setting this two λ_{max} using dual wavelength mode. Absorbance noted for each time samples and converted to concentration using corresponding Y

equation of linearity of standard Lawsone and *R. cordifolia* extract.

These concentrations enabled the calculation of cumulative drug release and permeation per cm² as Shown in Table 1.

Additionally, flux (J) and permeability coefficient (Kp) were calculated and shown in Table 2.

Flux (J) is the rate of drug passage through a membrane per unit area, calculated as: $J = \text{Slope} / \text{Area}$ (mg/cm²/hr).

The permeability coefficient (Kp), indicating membrane permeability, was derived from $Kp = J / C_0$ (cm/hr), where C_0 is the initial drug concentration. A graph of X axis-Time vs. Y axis- cumulative drug permeated per cm² was plotted for each analysis set for LIE and RCE, with comparative values for flux (J) and Kp. The highest flux and kp are selected for optimal diffusion.

Graphs for drug diffusion kinetic studies were plotted for the following kinetic models: Zero-order kinetic (% cumulative drug released against the Time), First-order (log cumulative drug remaining vs. Time), Korsmeyer-Peppas model (Log% cumulative drug released Vs. Log time), Higuchi model (% cumulative drug released vs. Square root of time), and Hixson-Crowell model (Cube root of % drug remaining vs. Time).¹⁵⁻¹⁹

The linear regression coefficient (R²) was used to determine the best fit kinetic model; the model was closest to one is the best fit.

RESULTS

The percentage cumulative drug release (% CDR) of Lawsone from *L. inermis* extract (LIE) and of *R. cordifolia* extract (RCE) from two different formulations *Shatadhauta Ghrita* based

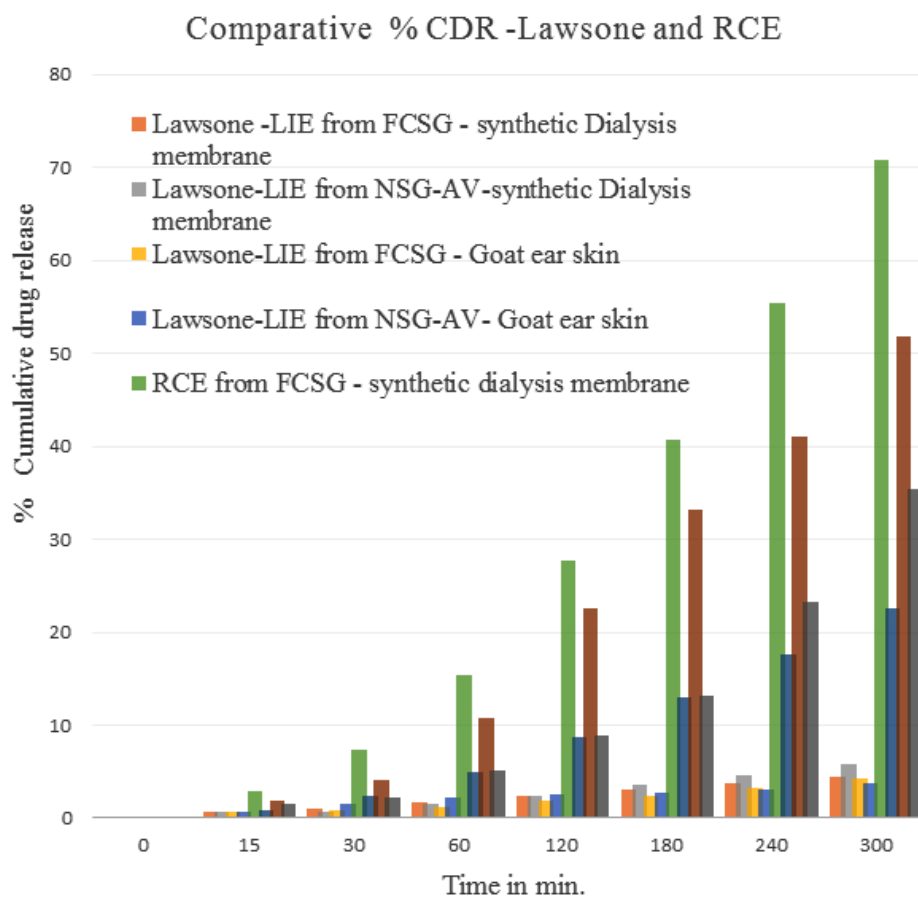


Fig. 1. Comparative % CDR through synthetic dialysis membrane and goat ear skin between Lawsone of LIE from FCSG and NSG-AV; and RCE from FCSG and NSG- AV

(FCSG) and Non- *Shatadhauta Ghrita* Aloe Vera gel based (NSG-AV) formulation using two types of membranes synthetic dialysis and biological are as shown in Table 1, and graph plotted as % CDR on Y axis and time on X axis for comparison of diffusion between membrane and formulation as shown in Fig. 1.

As per Fig. 1 regarding % CDR for Lawsone of LIE, the highest release is observed from Non- *Shatadhauta Ghrita* Aloe Vera gel (NSG-AV) using the synthetic dialysis membrane (~6% at 300 min) as compare to Foot Crack Cream *Shatadhauta Ghrita* (FCSG) shows slightly less release (~4.5%). Both formulations in goat ear skin membranes shows lower % CDR compared to synthetic membranes. However, FCSG shows slightly better release through goat ear skin compared to NSG-AV and is more consistent and linear in release

As per Fig. 1 regarding % CDR of RCE (*R. cordifolia* extract) highest cumulative release (~70%) is seen from Foot Crack Cream *Shatadhauta Ghrita* (FCSG) with synthetic dialysis membrane. FCSG with goat skin also shows better

release (~50%) than all Non- *Shatadhauta Ghrita* Aloe Vera gel (NSG-AV) groups. NSG-AV shows the least release, especially through goat skin (~30%) and synthetic membrane (~22%).

Flux, permeability coefficient (Kp), and lag time of Lawsone (from *L. inermis extract*, LIE) and Rubiadin (from *R. cordifolia extract*, RCE) were evaluated from FCSG and NSG-AV across synthetic dialysis and biological membranes as shown Table 2.

The dialysis membrane, Lawsone showed higher flux with the Aloe Vera-based formulation and slightly lower flux with the *Shatadhauta Ghrita* based formulation. However, when considering both membrane types overall, the highest flux was observed from the Ghrita based formulation. Similarly, the permeability coefficient (Kp) for Lawsone was highest through the goat skin membrane, although it exhibited a longer lag time likely due to its hydrophilic nature.

Secondly, in the dialysis membrane, RCE showed the highest flux and permeability Kp with the *Shatadhauta Ghrita* based formulation, along with a quick release and comparatively low

Table 1. Comparative % CDR through synthetic dialysis membrane and goat ear skin membrane between *FCSG, and *NSG-AV analyzed at λ max 452 nm (for Lawsone from *LIE) and at max 322 nm (for *RCE)

Time	% CDR for Lawsone from LIE			
	Synthetic Dialysis membrane		Goat ear skin	
	% CDR -FCSG (Cell-1)	% CDR -NSG-AV (Cell-3)	% CDR -FCSG (Cell-2)	% CDR -NSG-AV (Cell-4)
15	0.5353	0.3432	0.375996	0.504
30	1.084774	0.756	0.7848	1.5288
60	1.74951	1.4568	1.205604	2.2764
120	2.344774	2.3964	1.852404	2.6184
180	3.102669	3.5304	2.474004	2.7336
240	3.767405	4.596	3.2532	3.0564
300	4.50951	5.8368	4.217604	3.8136
	% CDR for RCE			
15	2.90143	0.92402	1.84	1.57
30	7.417144	2.36215	4.07	2.152857
60	15.42143	4.91128	10.80143	5.19
120	27.61143	8.79345	22.48143	8.944286
180	40.75143	12.97816	33.21429	13.21857
240	55.31429	17.61602	40.99	23.18
300	70.79	2.54459	51.87	35.32

*FCSG (Foot Crack Cream *Shatadhauta Ghrita*), *NSG-AV (Non *Shatadhauta Ghrita* Aloe vera gel), *LIE (*L. inermis* extract), *RCE (*R. cordifolia* extract)

lag time. While in biological membrane its flux, permeability and lag time are moderate average through Ghrita formulation.

The in vitro release kinetics of Lawsone and RCE (*R.cordifolia* extract) from two different formulations, were evaluated using various mathematical models, including Zero-order, First-order, Higuchi, Korsmeyer–Peppas, and Hixson–Crowell. The corresponding linear regression coefficient values (R^2) were calculated to determine the best-fitting release model for both formulations, as shown in Table 3. Fig. 2 (a) to (e) and Fig. 3 (a)

to (f) shows selected graphs for best fitting models through Synthetic dialysis membrane and goat ear skin membrane respectively for Lawsone and RCE.

DISCUSSION

Synthetic membranes allow higher permeation overall. Aloe Vera gel based formulation promotes better Lawsone diffusion through synthetic membrane, likely due to its hydrophilic nature. However *Shatadhauta Ghrita*

Table 2. Permeation parameters- Lawsone of *LIE and *RCE from *FCSG and *NSG- AV through Dialysis and Goat ear skin membrane

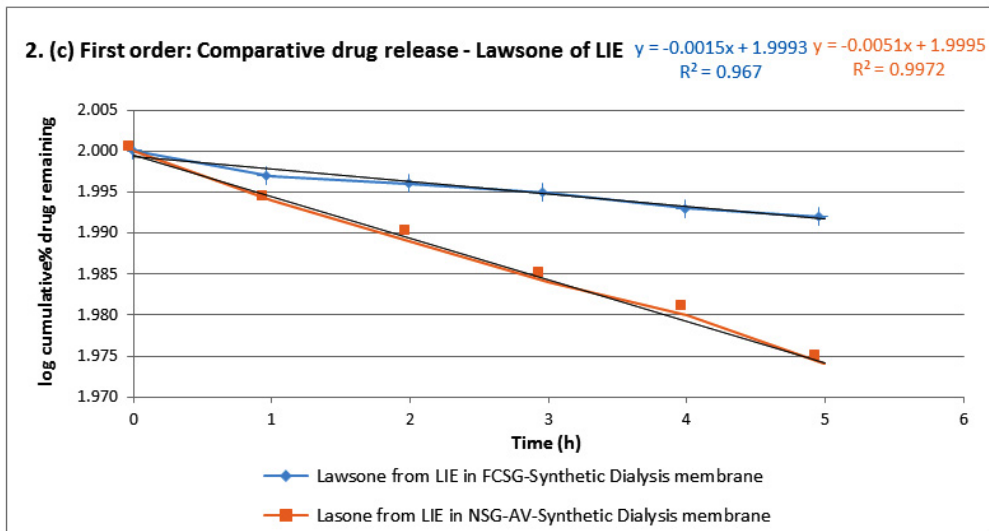
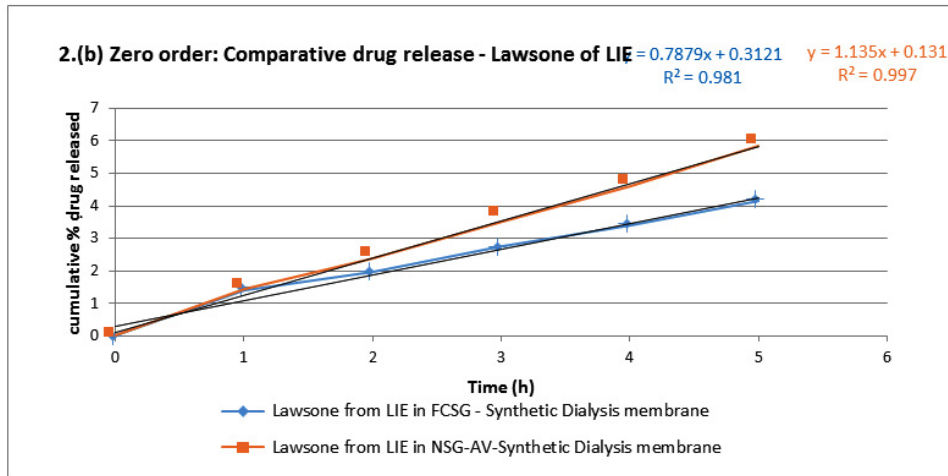
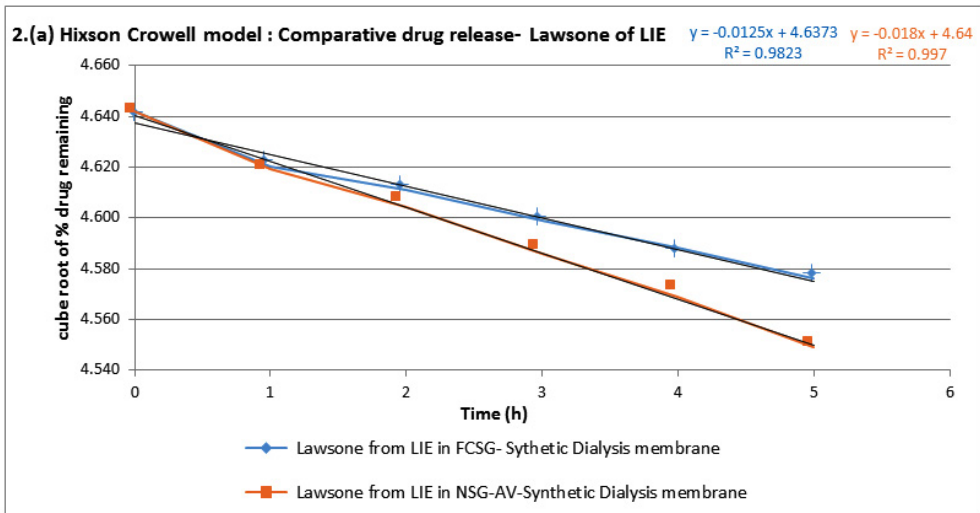
Membrane Type, λ max and molecule	Drug Formulation	Graph X axis = Time Vs Cumulative drug amount in mg	Flux (J) = Slope/Area (mg/cm ² /hr)	Permeability Coefficient (Kp) = J / C ₀ (cm/hr)	Lag Time min
Dialysis, 452 nm, Lawsone	FCSG	$y = 0.0221x + 0.0322$	0.00701	0.0007	10- 15
Goat ear skin, 452 nm, Lawsone	NSG-AV	$y = 0.0349x + 0.0088$	0.01083	0.00110	10
Dialysis, 322nm, RCE	FCSG	$y = 0.0742x + 0.0373$	0.0236	0.0035	20-25
Goat ear skin, 322nm, RCE	NSG-AV	$y = 0.0351x + 0.1846$	0.0111	0.00111	20-25
Dialysis, 452 nm, Lawsone	FCSG	$y = 0.186x + 0.687$	0.40892	0.0409	10-15
Goat ear skin, 452 nm, Lawsone	NSG-AV	$y = 1.384x + 0.044$	0.1866	0.0187	20-25
Dialysis, 322nm, RCE	FCSG	$y = 0.320x + 0.053$	0.10191	0.0102	15- 20
Goat ear skin, 322nm, RCE	NSG-AV	$y = 0.237x - 0.164$	0.00755	0.0076	25- 30

*LIE (*L.inermis* extract), *RCE (*R.cordifolia* extract), *FCSG (Foot crack cream *Shatadhauta Ghrita*), *NSG-AV (Non *Shatadhauta Ghrita*-Aloe vera), J *- Flux, Kp- Permeability coefficient, C₀ - initial drug concentration (10mg), Area=3.14 cm².

Table 3. Comparative kinetic modeling and best fit analysis - Lawsone of LIE and RCE release through Dialysis membrane and goat ear skin membrane

Metabolite	Zero order	First Order	Higuchi	Peppas	Hixson–Crowell	Best fitting model
Dialysis Membrane – Values of R²						
Lawsone from FCSG	0.981	0.967	0.969	0.962	0.982	Hixson
Lawsone from NSG-AV	0.997	0.997	0.929	0.969	0.997	Zero order, First Order, Hixson
RCE from FCSG	0.860	0.991	0.995	0.993	0.904	Higuchi
RCE from NSG-AV	0.998	0.959	0.974	0.996	0.979	Zero order
Goat Ear skin Membrane– Values of R²						
Lawsone from FCSG	0.989	0.989	0.939	0.983	0.989	Zero order, First order, Hixson
Lawsone from NSG-AV	0.940	0.909	0.772	0.825	0.920	Zero Order
RCE from FCSG	0.997	0.993	0.928	0.997	0.997	Zero order, PeppasHixson
RCE from NSG-AV	0.940	0.909	0.772	0.952	0.9205	Peppas

*FCSG (*Shatadhauta Ghrita* based foot crack cream), *NSG-AV (Non *Shatadhauta Ghrita*- Aloe Vera gel formulation), *LIE (*L.inermis* extract), *RCE (*R.cordifolia* extract)



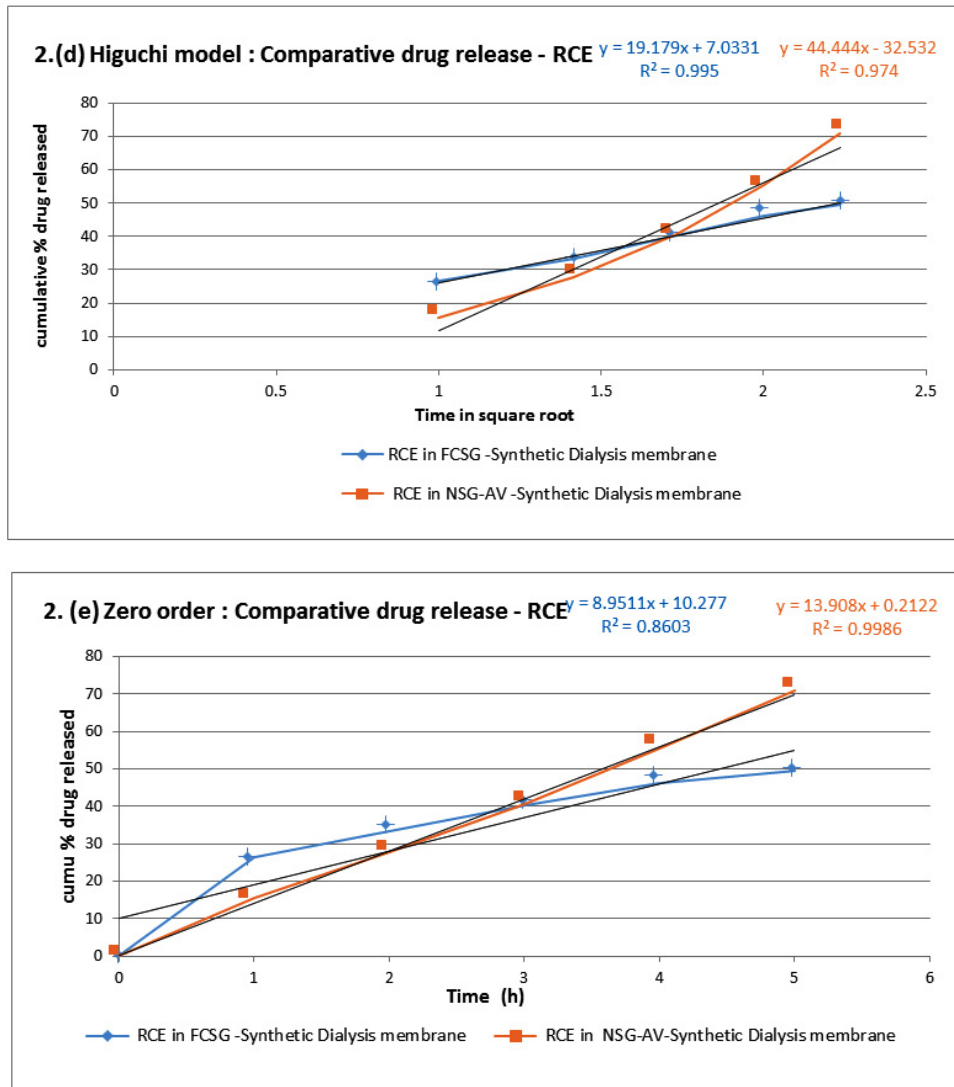
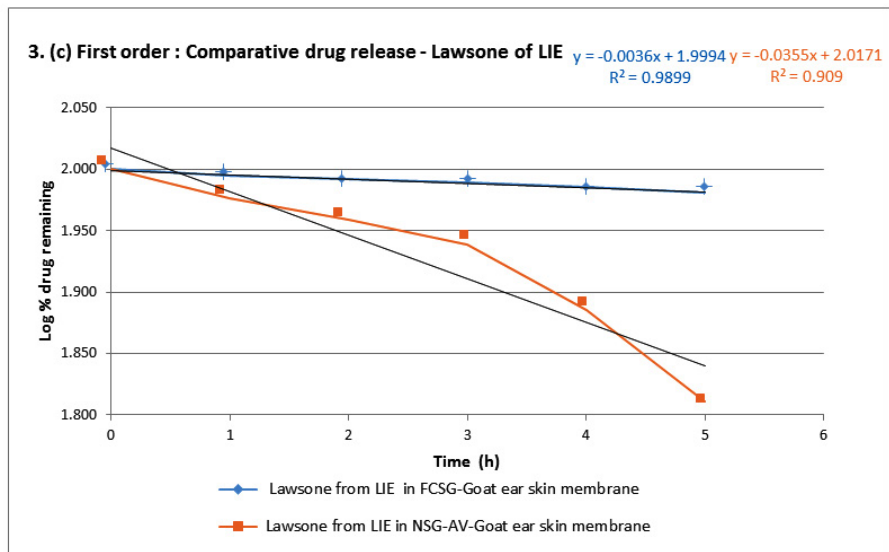
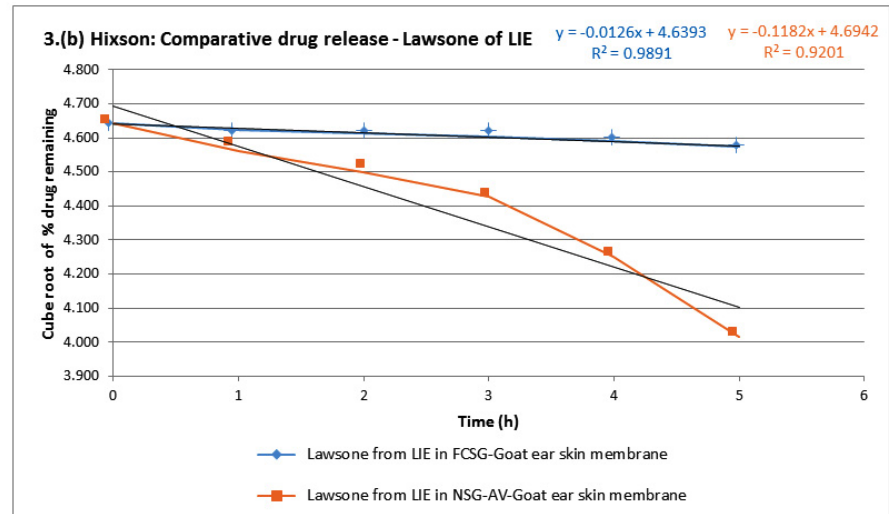
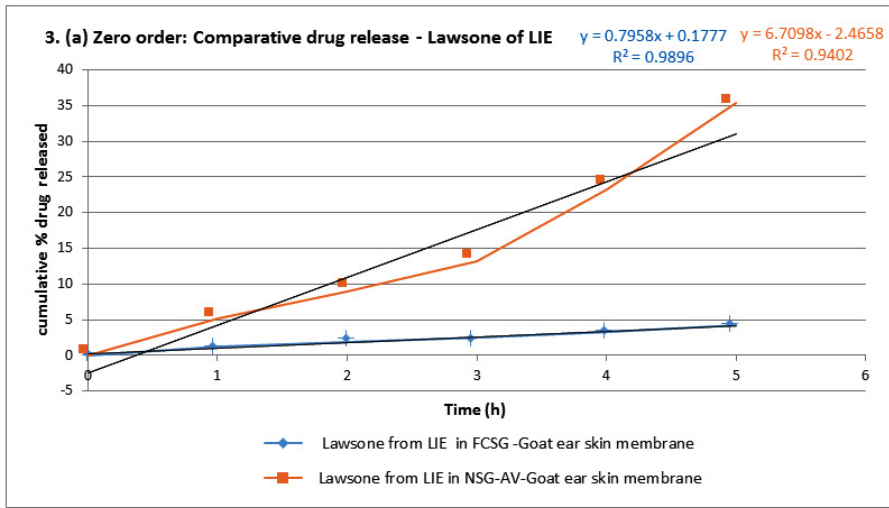


Fig. 2. Comparative Drug release best fit kinetic models of formulations FCSG & NSG-AV in synthetic dialysis membrane, (a) Hixson model of Lawsone, (b) Zero order of Lawsone, (c) First order of Lawsone, (d) Higuchi model of RCE (e) Zero order of RCE

based formulation (FCSG), enhances goat ear skin permeation of Lawsone compared to aloe vera base.

Shatadhauta Ghrita based formulation (FCSG) significantly enhances the release and permeation of RCE, especially for hydrophobic bioactives like Rubiadin. Goat ear skin shows a real skin barrier, so the enhanced performance of FCSG here confirms better transdermal potential. Aloe vera based formulation NSG-AV fails to deliver RCE effectively due to possibly poor lipid compatibility or insufficient permeation enhancer.

Therefore overall, a Diffusion insight shows that, Synthetic membranes offer less resistance and hence higher CDR values. Goat ear skin, being a biological barrier, offers a realistic model of human skin permeability. *Shatadhauta Ghrita* (FCSG) formulation improves diffusion across both synthetic and biological membranes, especially for lipophilic compounds like Rubiadin from RCE. Aloe vera may offer better delivery for hydrophilic drugs like Lawsone but is inferior for lipophilic compounds.



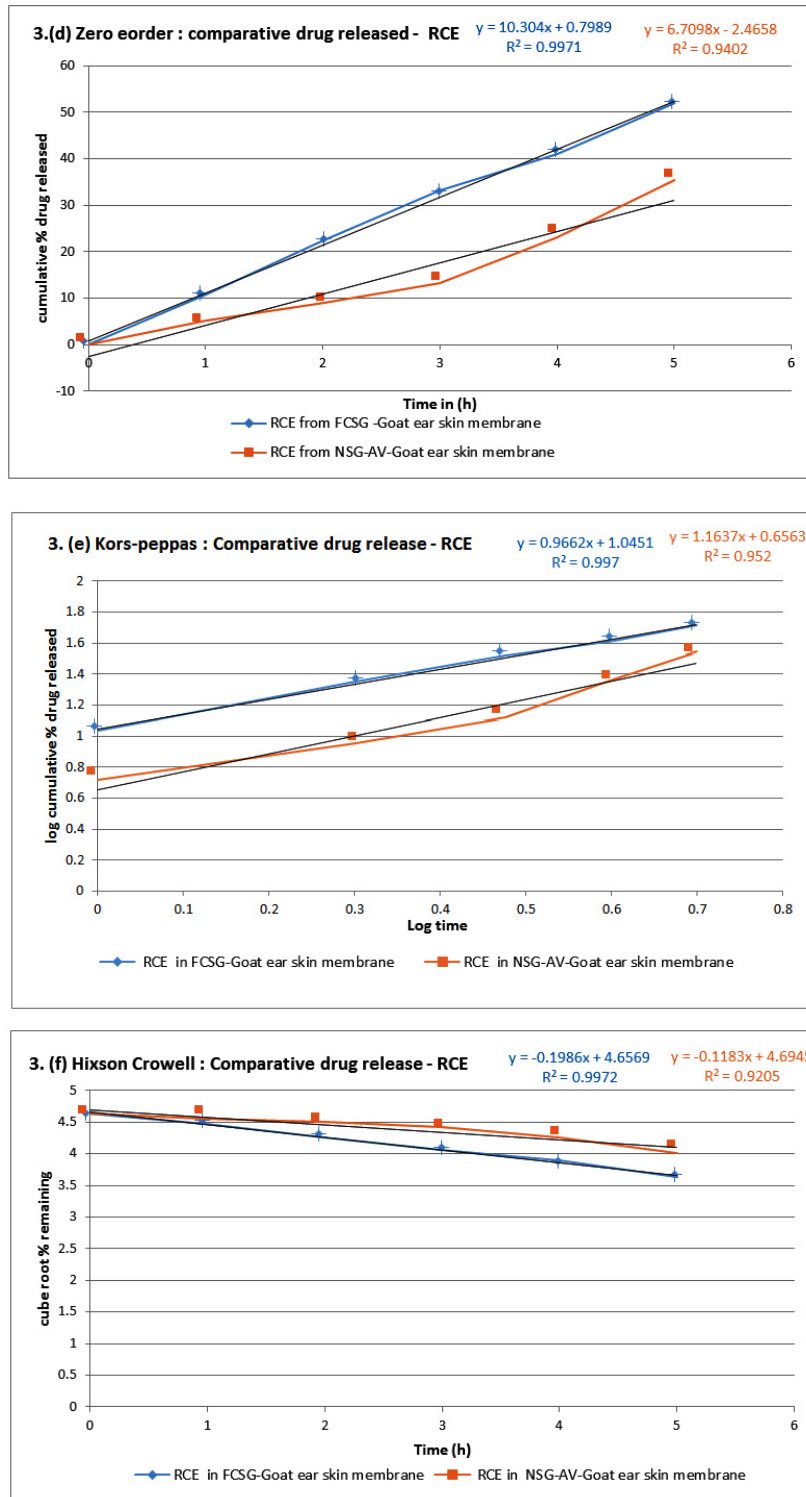


Fig. 3. Comparative Drug release best fit models of formulations FCSG & NSG-AV in Goat skin (a) Zero order of Lawsone, (b) Hixson of Lawsone, (c) First order of Lawsone, (d) Zero order of RCE (e) Kors-peppas of RCE, (f) Hixson Crowell of RCE

Due to Ghrita's better lipid solubility and transdermal effectiveness, *Shatadhauta Ghrita* formulation significantly increases RCE penetration into biological membrane as compared to NSG-AV, indicating enhanced transdermal delivery prospective.

However, *Shatadhauta Ghrita* based formulation showed consistently increased diffusion flux, permeability and moderate lag time, particularly across biological membranes making it more efficient for transdermal delivery of both bioactives Lawsone and Rubiadin. Aloe vera based formulation showed a faster onset in some cases but lacked sustained and efficient permeation.

Shatadhauta Ghrita based formulation (FCSG) maintained effective diffusion even across this barrier, demonstrating its therapeutic promise in contemporary skin diseases.

Kinetic modeling and best fit models

As per Table 3, the release of lawsone from the *Shatadhauta Ghrita* based formulation (FCSG) through the dialysis membrane predominantly followed the Hixson–Crowell model, indicating that changes in particle size and surface area due to matrix erosion play a major role in controlling drug release (Fig. 2.(a)). In contrast, release through the biological membrane (goat ear skin) exhibited higher correlation values for zero-order, first-order, and Hixson–Crowell models (Fig. 3.(a) to 3.(c)). This suggests that erosion acts as an initial release mechanism, followed by diffusion and a relatively constant drug release profile.

Although lawsone is hydrophilic in nature, its release from the aloe vera–based formulation (NSG-AV) through the dialysis membrane followed zero-order, first-order, and Hixson–Crowell kinetics (Fig.2.(b) and Fig.2.(c)), indicating a complex release mechanism involving continuous, concentration-dependent, and erosion-controlled processes. However, in goat ear skin, lawsone release from NSG-AV showed a higher correlation with the zero-order model (Fig.3.(a)), suggesting a more uniform and sustained release across the biological membrane.

For RCE, the Higuchi model provided the best fit for the *Shatadhauta Ghrita*–based formulation using the synthetic dialysis membrane, indicating that drug release was primarily governed by diffusion (Fig 2.(d)). In contrast, release

through goat ear skin followed both zero-order and Korsmeyer–Peppas models (Fig.3.(d) and Fig.3.(e)), suggesting a sustained release governed predominantly by Fickian diffusion through the skin barrier.

RCE release from the aloe vera–based formulation closely followed zero-order kinetics in the dialysis membrane (Fig.2.(e)), indicating a consistent drug release rate independent of concentration. In the goat ear skin membrane, the Korsmeyer–Peppas and Hixson–Crowell models (Fig.3.(e) and Fig.3.(f)) showed moderate correlation, suggesting that although diffusion and erosion contribute to the overall release process, their contribution is secondary to the dominant zero-order release mechanism.¹⁸⁻²⁵

CONCLUSION

This research demonstrates, the *Shatadhauta Ghrita* based formulation provides considerably better topical delivery of bioactive compounds such as Lawsone and Rubiadin than the Non-*Shatadhauta Ghrita* Aloe Vera gel based formulation. The *Shatadhauta Ghrita* based formulation showed higher flux with better permeability and sustained release across both membranes Synthetic and goat ear skin. The kinetic modeling indicates that Lawsone follows a controlled release mechanism involving both diffusion and matrix erosion, while Rubiadin exhibits a sustained, Fickian diffusion driven release. The lipid rich *Shatadhauta Ghrita* base effectively supports the dual release behavior, enhancing the delivery of both phytoconstituents. These results showed that the traditional use of *Shatadhauta Ghrita* as a scientifically reliable and effective carrier for herbal bioactives, making it a potential natural alternative for the topical treatment of cracked heels and other skin conditions. The result demonstrates that the *Shatadhauta Ghrita* enhances the dermal drug delivery, provides a scientifically verified base for natural therapeutic foot care application.

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The authors do not have any conflict of interest.

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This statement does not apply to this article.

Ethics Statement

This research did not involve human participants, animal subjects, or any material that requires ethical approval.

Informed Consent Statement

This study did not involve human participants, and therefore, informed consent was not required. Clinical Trial.

Clinical Trial Registration

This research does not involve any clinical trials.

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Not Applicable.

Author Contributions

Daksha Lalit Attarde : Conceptualization, Methodology, Data Collection, Investigation, Writing, Review, Editing and Supervision; Sulochana Sonya Gavit : Conceptualization, Literature review, Methodology, Formal analysis, Investigation, Data Collection, Writing; Bhagyashree Nanasaheb Borde : Literature review, Data Collection, Writing, Review and Editing,

traditional knowledge: incorporating cow ghee and shata dhauta ghrita in modern moisturizing creams. *World J Pharm Res.* 2025;14(1):649–660. doi:10.20959/wjpr20251-35152

5. Nadkarni KM. *Indian Materia Medica*. 3rd ed. Mumbai: Popular Prakashan. 2002; vol 1:714-716,1062-1065.
6. Batiha GE, Teibo JO, Shaheen HM, et al. Therapeutic potential of Lawsonia inermis Linn: a comprehensive overview. *Naunyn-Schmiedeberg's Arch Pharmacol.* 2024;397(6):3525-3540. doi: 10.1007/s00210-023-02735-8.
7. Khare CP. *Pharmacopoeal and Related Drugs of Biological Origin*. New Delhi: Business Horizons. 2005;293-295, 367-369.
8. The Wealth of India. New Delhi: Council of Scientific and Industrial Research. 1972;vol 9:288-292.
9. Indian Pharmacopoeia. Ghaziabad: Indian Pharmacopoeia Commission. 2022;vol I:1064, vol.III:1354.
10. Kakad S, Bajpai N. Manjistha (*Rubia cordifolia*): A herbal treasure of India. *Int J Multidiscip Res.* 2024;6(4):1-9. doi.org/gt3ngf.
11. Singh B, Dadhich OP, Deepa. A review study of medicinal uses of Manjistha (*Rubia cordifolia*). *Int J Adv Res.* 2017; 5(8):1394-1401. doi:10.21474/IJAR01/5196.
12. Evans WC. *Trease and Evans Pharmacognosy*. 16th ed. Edinburgh: Saunders Elsevier. 2009;545-547.
13. Deshmukh MD, Patil MP, Ahire ED, Gosavi SB. Shatdhauta ghrita: A promising agent in the development of herbal creams. *J. Pharm. Negat. Results.* 2022;13(S1):1332–1343. doi:10.47750/pnr.2022.13.S01.159.
14. Kumar M., Sharma A., Mahmood S., Thakur A., Mirza MA., Bhatia, A. Franz diffusion cell and its implication in skin permeation studies. *Journal of Dispersion Science and Technology*, 2024;45(5): 943–956. doi.org/10.1080/01932691.2023.2188923
15. Askarizadeh M, Esfandiari N, Honarvar B, Sajadian SA, Azdarpour A. Kinetic modeling to explain the release of medicine from drug delivery systems. *Chem Bio Eng Rev.* 2023;10(6):1006–1049. doi.org/10.1002/cben.202300027
16. Siepmann J, Siepmann F. Mathematical modeling of drug delivery. *Int J Pharm.* 2008;364(2):328–343. doi.org/10.1016/j.ijpharm.2008.09.004.
17. Earle RR, Bandaru KK, Lakshmi UA. Formulation and characterization of sustained release coated matrix granules of metformin hydrochloride. *Asian J Pharm Clin Res.* 2018;11(7):387-392. doi.org/10.22159/ajpcr.2018.v11i7.24996.
18. Jahromi PL, Ghazali M, Ashrafi H, Azadi A.

REFERENCES

1. Sanap TD, Pawar JR. Review on heel fissure and their management. *J. Emerg. Technol. Innov. Res.* 2024;11(11). doi:10.6084/m9.jetir.jetir2411441.
2. Hashmi F, Wright C, Nester C, Lam S. The reliability of non-invasive biophysical outcome measures for evaluating normal and hyperkeratotic foot skin. *J Foot Ankle Res.* 2015;8(1):28. doi: 10.1186/s13047-015-0083-8.
3. Wyal SR, Gurav SS. Bhallatakadi Ghrita: Development and evaluation with reference to Murcchana and Shata-Dhauta process. *J Ayurveda Integr Med.* 2020;11(3):261-269. doi.org/10.1016/j.jaim.2020.05.005.
4. Chhangani JA, Kathale PS, Agnihotri AK, Murkute AA, Katre SG. A review on utilizing

- A comparison of models for the analysis of the kinetics of drug release from PLGA-based nanoparticles. *Heliyon*. 2020;6(2):e03451. doi.org/10.1016/j.heliyon.2020.e03451.
19. Mahshid A, Nadia E, Bizhan H, Seyed Ali S, Amin A. Kinetic modeling to explain the release of medicine from drug delivery systems. *Chem Bio Eng Rev*. 2023;10(6):1006-1049. doi.org/10.1002/cben.202300027.
20. Lachman L, Lieberman HA, Kanig JL. *The Theory and Practice of Industrial Pharmacy*. 3rd ed. Mumbai: Varghese Publishing House. 1991.
21. Simona A, Amaro MI, Healy AM, Cabral LM, Sousa VP. Comparative evaluation of rivastigmine permeation from a transdermal system in the Franz cell using synthetic membranes and pig ear skin with in vivo–in vitro correlation. *Int J Pharm*. 2016;512(1):234-241. doi.org/10.1016/j.ijpharm.2016.08.052.
22. Kumar M, Sharma A, Mahmood S, Thakur A, Mirza MA, Bhatia A. Franz diffusion cell and its implication in skin permeation studies. *J Dispersion Sci Technol*. 2023;45(5):1-14. doi.org/10.1080/01932691.2023.
23. Torlak C, Guleli M, Kizilok S, Kartop RA, Caliskan C, Baysak FK. Comparison of permeability of topical cream drug through polymer synthetic membranes of different structures using Franz Cell diffusion test. *J Dispersion Sci Technol*. 2024;45(14):1-9. doi.org/10.1080/01932691.2024.2390970.
24. Kim KM. A Study of the Transdermal Permeation of Lotion Formulations containing Angelica gigas Nakai Extracts in Franz Diffusion Cells. *J Life Sci*. 2021; 31(11): 1004-9. doi.org/10.5352/JLS.2021.31.11.1004
25. Liebenberg W, Engelbrecht E, Wessels A, Devarakonda B, Yang W, De VM. A comparative study of the release of active ingredients from semisolid cosmeceuticals measured with Franz, enhancer or flow-through cell diffusion apparatus. *J Food Drug Anal*. 2004;12(1):10 . doi.org/10.38212/2224-6614.2669